

Webinar #3

Lattice Boltzmann method for CompBioMed (incl. Palabos)

19 March 2018

The webinar will start at 12pm CET / 11am GMT



Dr Jonas Latt (Head of Research, University of Geneva)

This project has received funding from the European Union's Horizon 2020 research and innovation programme under grant agreement No 675451

The series is run in collaboration with:





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19 March 2018 Welcome!



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Today's topics

- The role of Computational Fluid Dynamics in biomedical modelling.
- Presentation of the Lattice Boltzmann Method.
- Two application examples of our tool Palabos in Computational biomedicine.

Example: treatment of aneurysms



Image by Lucien Monfils

Angiography of an aneurysm in a brain artery.

Flow Diverters



Insights from computer simulations

Simulations show aneurysm Wall-Shear-Rate (WSR) deciding factor for thrombus formation.



J NeuroIntervent. Surg. 2015, 011737



Patient-specific aneurysm treatment



1. Medical knowledge



2. Expertise in (molecular) biology



1. Medical Knowledge

Anchoring of bovine prothrombin to the membrane

Image by Andrei Lomize

3. Numerical Modeling



1. Medical Knowledge

2. Expertise in (molecular) biology

4. Computer Programming

1. Medical Knowledge

2. Expertise in (molecular) biology

3. Numerical Modeling

5. High Performance Computing



Piz Daint Supercomputer, CSCS (Switzerland)

1. Medical Knowledge

2. Expertise in (molecular) biology

3. Numerical Modeling

4. Computer Programming



Today's topic: Computational Fluid Dynamics

Computer solution to fluid flow equations (so-called Navier-Stokes equations).

Examples of fluids:

. . .

- The blood or blood plasma in an artery.
- The air in the lungs.
- The Cerebrospinal fluid.
- Fluids used by doctors in medical interventions.

Today's method: Lattice Boltzmann Method

- Modern approach to Computational Fluid Dynamics.
- Particularly useful for complex, coupled physical systems (e.g. representation of Red Blood Cells in the blood plasma).
- Adjusts in a simple manner to the requirements of high performance computers.

Technical part of the Webinar: Intro to Lattice Boltzmann Method

- Technical, precise introduction with reference to actual code.
- A simple, illustrative program in the Python language is provided alongside with this Webinar.
- No previous knowledge required!

Background: Lattice Gas Automata



- HPP: A model from the 1980ies.
- Goal: represent a gas by modeling individual, yet highly simplified gas molecules.
- Space is discretized: represented by individual cells.
- Boolean model: each cell has between
 0 and 4 «molecules», traveling in 1 one
 the main directions.

Lattice Gas Automata: Model

- When several particles meet on a node, they collide: all physics takes place here.
- After collision, particles are streamed to a nearest neighbor.





Poll time!

Please respond to the poll that will appear on the screen

Starting from Cellular Automata, how could simulation speed be improved substantially?

Right Answer: By replacing a discrete model by a statistical one.

From discrete to continuum variables



In a lattice gas automaton:

- Run the simulation with discrete variables.
- At the end, extract macroscopic variables by taking averages.

Lattice Boltzmann Method: Idea



- Run simulation with continuum variables right away, to save space.
- Continuum model is derived from discrete method by means of statistics.
- Particle density: real-valued.
- Arrow thickness stands for particle density.

Lattice Boltzmann Method: details



Lattice Boltzmann 2D model D2Q9:

- Four directions aren't quite enough.
- Nine directions: eight connections to nearest neighbors + «rest population».
- Variables representing particle densities are called «populations».

Lattice Boltzmann Variables



Space Discretization:

- Every cell represents flow variables at a point in space.
- To represent space with 8x8 points, we need a total of 8x8x9 = 576 floating point variables.
- Equal distance δx between cells in xand y-direction.

Python code to allocate memory:

Collision step



- Like lattice gas: maps pre-collision to post-collision populations.
- All populations are modified during collision. Changes are not visible on video, because they are small perturbations.

Our color scheme:



Collision step



Model:

- Collision is instantaneous.
- Collision is localized at cell coordinates.

Our color scheme: Green: pre-collision Red: post-collision

Streaming step



Model:

- Streaming takes the system from time t to time $t + \delta t$.
- Streaming includes nearestneighbor access.

Our color scheme:



Pre- and post-collision: variables

In our Python code, we save incoming and outgoing populations in separate matrices.



Python code:

assign some size
nx, ny = ...
fin = zeros(9, nx, ny)
fout = zeros(9, nx, ny)

Density

Each cell has its own density, which is the sum of the nine populations.

Equation

Python Code

$$\rho(\boldsymbol{x},t) = \sum_{i=0}^{8} f_i^{\text{in}}(\boldsymbol{x},t)$$

rho = sum(*fin*, axis=0)

Pressure

Pressure is proportional to density, like in an ideal gas:

$$p = c_s^2 \rho$$

- Blood is not a gas, it is incompressible: Density is constant.
- We still solve for a quantity we call "density", just as a trick to compute the pressure cheaply.

Velocity

Let's introduce a set of 9 vectors:



Velocity is a weighted sum of the populations:

$$\boldsymbol{u}(\boldsymbol{x},t) = \frac{1}{\rho(\boldsymbol{x},t)} \frac{\delta x}{\delta t} \sum_{i=0}^{8} \boldsymbol{v}_{i} f_{i}^{\text{in}}(\boldsymbol{x},t)$$

Python code:

u = zeros((2, nx, ny))
for i in range(9):
 u[0,:,:] += v[i,0] * fin[i,:,:]
 u[1,:,:] += v[i,1] * fin[i,:,:]
u /= rho

Collision: BGK model

Collision is a relaxation to local equilibrium:

$$f_i^{\text{out}} - f_i^{\text{in}} = -\omega \left(f_i^{\text{in}} - E(i, \rho, \vec{u}) \right)$$

- *E*: local equilibrium. Depends on the macroscopic variables and has a different value for every direction *i*.
- ω : frequency of relaxation, relates to the fluid viscosity.

Collision: Python code

Collision formula:

$$f_i^{\text{out}} - f_i^{\text{in}} = -\omega \left(f_i^{\text{in}} - E(i, \rho, \vec{u}) \right)$$

Python program:

fout = fin - omega * (fin - eq)

Streaming step

Time *t*

Time $t + \delta t$

Streaming takes the system to the next time iteration, $t + \delta t$



Streaming step: code

Python code:

for i in range(9):
 fin[i,:,:] = roll(
 roll(fout[i,:,:], v[i,0], axis=0),
 v[i,1], axis=1)

The Palabos software



- Developed at University of Geneva.
- Our tool for biomedial fluid dynamics: all examples today run by Palabos.
- Open-Source: www.palabos.org

Another simulation example

Vertebroplasty:

Treatment of compression fractures in a vertebra.



Image: Blausen.com staff

Micro-CT: porous bone structure



Computer simulation



Experiment vs. Simulation: Case 1

After 3 milliliters







Simulation

Can we do « real time »?





Poll time!

Please respond to the poll that will appear on the screen

Which trick made this simulation substantially faster?

Right Answer: Allocate only areas filled by cement, dynamically

A better idea: sparse memory



A better idea: sparse memory



Sparse-Mem 3-4 times faster



Many thanks to ...

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Further Resources

Palabos Web Page:

www.palabos.org

A more thorough course:

https://www.coursera.org/learn/modeling-simulationnatural-processes





To pose a question, you can:

- 1. if you have a microphone, raise your hand and we will unmute you, when it is your turn to speak or
 - 2. write your question in the "Questions" tab



Thank you for participating!

Visit the CompBioMed website (<u>www.compbiomed.eu/training-3</u>) for a full recording of this and other webinars, to download the slides and to keep updated on our upcoming trainings

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